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Kanagawa-ken 248(JP)(64) **MICROELECTRODE FOR ELECTROCHEMICAL ANALYSIS.**

(57) A plurality of carbon fibers (1) are covered with an electrically nonconductive resin (2) so that the individual carbon fibers will not be brought into contact with each other, thereby forming a bundle of carbon fibers. Tips of the carbon fibers are retracted on one side of the carbon fiber bundle to form fine holes (3) that are open to the external side. If necessary furthermore, the retracted tips of the carbon fibers are coated with a permselective membrane, an enzyme or a microorganism, or an electrochemical catalytically active substance (4). The obtained microelectrodes have a small flow-rate susceptibility, undergo less contamination, and can be used as electrodes for measuring dissolved oxygen, as electrodes for measuring ion concentration, as electrodes for biosensors, or as reference electrodes.

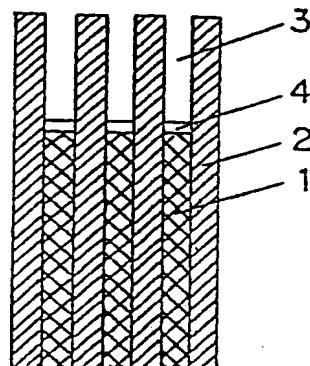


FIG. 1

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## THE MINUTE ELECTRODE FOR ELECTROCHEMICAL ANALYSIS

## TECHNICAL FIELD

This invention relates to the improved minute electrode such as dissolved oxygen measuring electrode, ion concentration measuring electrode, for bio-sensors and for reference electrode which has low flow sensitivity and also it protects from contamination.

## BACKGROUND ART

The analysis of oxygen, saccharide, amino acid, pH etc. has hitherto done by electrochemical method, using several kinds of electrodes. Following is the explanation of prior technique for various kinds of electrodes and sensors.

(1) The sensor for measuring the concentration of the dissolved oxygen

It is important to measure the concentration of the dissolved oxygen in the body fluid such as blood, or that of culture fluid in a fermenter jar. Clark type oxygen sensor has been used widely. Composition of this sensor is as follows.

The container of sensor is fulled by electrolyte such as caustic alkaline solution etc., and the cathode (for example made of platinum) and the anode (for example made of lead etc.) are set therein, and separated from outside (the solution which should be measured) by the gas permeable membrane made of polytetrafluoro ethylene etc.. The concentration of oxygen can be determined by measuring the electric current between two electrodes, whereas oxygen molecule passes from test solution to inside of the sensor container through selective permeable membrane, and it is reduced electrochemically on platinum electrode surface. By the appearance of this method, amount of oxygen can be determined easily, but there are still following problems. That is, instability for pressure at sterilization, difficulty for maintenance, limitation for miniaturization, and it can't determine the real dissolved oxygen concentration, but partial oxygen pressure, it can't determine the dissolved oxygen concentration in fermentation under pressure or can't determine it on the bottom of the sea and the lakes, and the variation of the electric current is rather big in accordance with temperature change.

Following methods are proposed for other oxygen concentration measuring electrodes, especially for body fluids. That is, the method to make the condition of

stable contact by means of covering the fine metal wire electrode surface with porous materials consisted of many layers (see Japanese Unexamined Patent Publication No.57-117838). And the method to insert the fine metal wire electrode into the opened tube in the recessed position from the tip of the said electrode (see Japanese Unexamined Patent Publication No.57-195436).

However, these methods have still following problems such as contamination of the electrode and the possibility to suffer from iatrogenic disease by peeling off the porous membrane.

(2) The sensor for measuring the concentration of ions

The glass electrode has been widely used for measuring the concentration of hydrogen ion. However, it has following several problems. That is, it is easy to break, also it is easy to contaminate, and it has the limitation using in the alkali aqueous solution. Moreover, it is very difficult to miniaturize, whereas the glass electrode needs the inside standard solution compartment. And there is a possibility that inside standard solution flows out.

Recently, following phenomena is discovered.

The membrane which is deposited by means of electrochemical polymerization on the surface of the electrode, causes the change in potential in accordance

with bonding or removing of the hydrogen ion. [William R. Heineman, Anal. Chem. 52, 345 (1980)] The following pH sensor is also proposed. The method has applied following phenomena that the membrane, which is formed on the surface of an electrode, causes reversible oxidation/reduction reaction with bonding or removing of hydrogen ion (see Japanese Unexamined Patent Publication No.61-19434). However, when these pH sensors are used continuously in the body fluids or fermentative solution, the potential drift is occurred in accordance with contamination.

### (3) Bio-sensor

There are two types of bio-sensors. That is, the first one is to determine the concentration of materials related to biochemical reaction, by measuring the current which caused in electrochemical reaction of said materials.

The another one is to analyse the electroactive materials (related to biochemical reaction), by measuring the potential of the membrane which selectively responds to said materials. The former one is called "Amperometry method" and in this case, oxygen sensor and hydrogen peroxide electrode are applied. On the other hand, the latter one is called "Potentiometry type" and ion selective electrode and ammonia or carbon dioxide gas

electrode (which consists of some kind of gas permeable membrane and pH electrode) are applied.

Enzyme, microorganism, and antigenantibody reaction are one of the biochemical reactions. The bio-sensor has problems said hereinbefore, whereas fundamental composition of bio-sensor is oxygen sensor or pH electrode.

#### (4) The reference electrode

Conventional reference electrode has following problems; 1) it is easy to break, 2) it is hard to ensure for the pressure of sterilization, whereas the saturated calomel electrode and silver/silver chloride electrode etc. includes inside-solution.

Therefore, the object of the present invention is to provide the various type of electrodes and also sensors which can determine for example, the dissolved oxygen, saccharide, amino acid, pH etc. stably and accurately without disadvantage of prior techniques.

#### DISCLOSURE OF THE INVENTION

The present invention relates to the minute electrode for electrochemical analysis which is characterized in that it is comprised of carbon fiber bundle covered with nonconducting resin, and the end of carbon fiber is

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recessed from one end of said bundle, and the microholes released to the outside are made on the carbon fibers.

The minute electrode which has low flow sensitivity and protects from electrode contamination by interference substances can be obtained in accordance with this composition.

#### BRIEF DESCRIPTION OF THE DRAWINGS

The FIG. 1 shows the conceptual illustration of minute electrode of present invention, and FIG. 2 shows the conceptual illustration of the electrode for bio-sensor which is one of the definite application of this invention. The FIG. 3 shows the contamination by interference substances of each electrode which has micro-holes, and which has not, this has been carried out in Example 4.

#### BEST MODE FOR CARRYING OUT THE INVENTION

Conceptually, the minute electrode of this invention is shown in FIG. 1. The bundle of carbon fibers consist of plural carbon fibers 1 and nonconducting resin 2. In the same FIG. 1, the top of carbon fiber 1 is recessed from the top of nonconducting resin 2 and forms the micro-hole 3 which is released outside. And the bottom of this micro-hole which is the top part of carbon fiber becomes the

electrode surface. If desired, surface of the electrode may be modified by electrocatalyst 4 for electrochemical reactions. This electrode is hereinafter referred to as "basic electrode".

Though there is no limitation for carbon fibers which forms the basic electrode, following carbon fibers such as polyacrylonitrile based, pitch based, rayon based, phenol resin based etc. and also the one which is produced by vapour deposition method, is used preferably.

The nonconducting material is preferably selected from fluorinated resin, polyester resin, epoxy resin, polyphenyleneoxide resin, polyphenylenesulfide resin, urethan resin, silicon resin, vinylchloride resin, phenol resin etc.. When the minute electrode is used in the living body, high quality anti-thrombogenesity resin is most preferable.

The plural carbon fibers are covered with nonconducting resin, and it is subjected to heat-set process in order to be one body. The cross-section of that (body) is like islands (each carbon fiber) in the sea (the nonconducting resin). Namely, carbon fibers do not contact with each other. The number of the carbon fibers is usually in the range of from 50 to 50,000, and it is selected on purpose for use. And when this electrode is used as reference electrode, sometimes more than 50,000 of carbon fibers may

be used.

Generally, the ratio of the carbon fiber's area in the cross-section of this electrode is in the range of from 3 to 60%. The diameter of the carbon fiber is less than 20  $\mu\text{m}$ , and more preferably it is less than 10  $\mu\text{m}$ .

The diameter of carbon fiber is that of micro-hole and in case of less than 20  $\mu\text{m}$ , it causes so called "filter effect".

Generally, the depth of the micro-hole is in the range of from 0.5 to 500  $\mu\text{m}$ , and more preferably it is in the range of from 20 to 400  $\mu\text{m}$ . It is no problem, for example, if it is sharp like a pencil or in opposition it is hollowed. But in this case, the depth of the micro-hole is defined by the deepest part of it.

If desired, the surface of the electrode is coated with electrocatalyst. And that material may be selected from platinum, silver, gold, iridium, phthalocyanine and its derivatives etc.. The ability of oxygen reduction catalysis becomes higher in accordance with making this layer.

The basic electrode in this invention keeps more toughly from contamination by means of covering electrode surface with selective permeable membrane. It is desirable that this membrane is a polymer made by electrochemical polymerization.

For example, the basic electrode in this invention can be obtained by the following procedure.

At first, the bundle of the carbon fiber is impregnated with nonconducting resin which includes hardening agent, then the bundle is subjected to heat treatment process in order to harden the resin. In this way, wire like carbon fiber bundle which is covered with nonconducting resin is obtained. Then the carbon fiber bundle is cut for desired length, then one end of this bundle is burnished, and the lead wire is bonded by using silver paste to the other end. On the burnished side of the bundle, the micro-holes are formed by etching the carbon fibers by means of electrochemical oxidation which illustrates hereinafter.

Electrolytic solution may be selected from acid or alkaline solution, and alcohols such as methanol which includes supporting electrolyte. Then the anodic oxidation is done. In this process, the carbon fiber is connected to the anode, and the metal electrode is used as a counter electrode. The oxidation voltage is preferably in the range of from 1 to 100 volt. Also it is preferable method that the oxidation and reduction are repeated by turns.

When the surface of the electrode is coated with the electrocatalyst, following method such as plating, vacuum evaporation, sputtering etc. is applicable.

Including the basic electrode and also for other electrodes, the micro-hole may be filled up with gelatinoid material. Gelatinoid materials may be selected from agar, gelatin, polyacrylamide gel etc..

Various electrodes of the present invention are illustrated below more concretely.

(1) The electrode for measuring the concentration of dissolved oxygen.

Basic electrode itself may be applied as the electrode for measuring the concentration of dissolved oxygen. But more preferably, the surface of the basic electrode is coated with selective permeable membrane by electrochemical polymerization process. The best method of electrochemical polymerization is as follows. The supporting electrolyte such as sodium perchlorate, sodium sulfate is dissolved in the organic solvent such as acetonitrile etc. or water, and the monomer compound which should be electrochemically polymerized is added in it and then this mixed material is electrochemically polymerized at constant potential of 1 to 1.5 volt. There is no limitation, if the polymer doesn't have electroactivity and also it is the selective permeable membrane which protects from contamination. Monomer compound usable for present invention is selected from amino-containing aromatic compound or hydroxy aromatic compound for

example, 4,4'-diaminodiphenylether, 4,4'-diaminodiphenylsulfide, phenol, aniline, or phenol derivatives, aniline derivatives. In accordance with polymerization conditions, the electroactive membrane will be formed. For example, when aniline is used as monomer, alkaline or neutral condition should be adopted, otherwise the membrane has electroactivity.

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Repeating polymerization is preferable, whereas it makes the membrane coating complete and also makes the selective permeability higher.

When the oxygen sensor is made by using said electrode, silver/silver chloride is combined as counter electrode. This electrode may be applicable not only for measuring the dissolved oxygen but also for that of other electrochemical reactant materials, by means of changing the selective permeability.

## (2) The ion electrode

The ion electrode is covered with the membrane, which is electrochemically deposited on the basic electrode and responds to hydrogen ion. Hydrogen ion responsable membranes are electropolymerized membranes such as 2,6-dimethylphenol, 4,4'-biphenol, 1,2-deaminobenzen, 1-aminopyrene, 1,8-diaminonaphthalene, 1,5-diaminonaphthalene etc..

In order to measure the concentration of hydrogen ion, this electrode is dipped together with reference electrode such as the saturated calomel electrode into the solution, and the voltage between two electrodes is measured.

### (3) Bio-sensor

FIG. 2 shows the electrode for bio-sensor. The said electrode is covered with membrane 6, in which enzyme or microorganism 5 is immobilized.

Or those are immobilized on the inside surface of microholes 2.

In the case of potentiometry method, enzyme is selected from urease, penicillinase, glucoseoxidase, lipase etc.. And in the case of amperometry method, that is selected from glucoseoxidase, latic acid oxidase, L-aminooxidase, xanthionoxidase, uric acid oxidase, pyruvate oxidase, lactate oxidase etc. each kind of oxidasic enzyme.

Immobilized membrane 6 is selected from polyvinyl chloride, polyacrylamide, acetylcellulose, cellulose triacetate, cross linked polyvinylalcohol etc. Not only membrane but also fiber mass of nylon or its mesh may be applicable.

Enzyme or microorganism is immobilized with membrane by means of adsorption or inclusion, or making the covalent linkage, or making the cross link by gultaraldehyde.

In the case the enzyme or microorganism is immobilized onto the inside surface of the micro-hole of nonconducting materials, the enzyme is bonded to the functional group(amino group, for example) of the epoxy resin. In order to make bio-sensor, enzyme immobilized electrode and the counter electrode of silver/silver chloride are combined.

#### (4) Reference electrode

In the case of the reference electrode, silver and silver halide are deposited on the basic electrode surface. Chlorine and bromine are preferable as halogen. More preferably micro-holes are filled with gelatinoid material, as mentioned hereinbefore. And it is most preferable that the salt with halogen ion can be included in the gelatinoid material. Examples of the present invention and comparative examples are illustrated below.

## Example 1, 2, 3 and Comparative Example 1

The bundle of one thousand of carbon fibers ("Torayca T-300 1K", having the diameter of  $7\mu\text{m}$ ) was impregnated with the epoxy resin including the hardening agent.

This impregnated bundle of fibers was hardened after heating under being stretched, so the composite material like a wire having diameter about 0.3 mm was obtained.

After the side face of this wire was insulated by epoxy resin completely, it was cut. And the one cross sectional face was burnished by the conventional method, and another end was bonded to the lead wire by silver paste, then the electrode was made.

This burnished part was dipped in the sulfuric acid aqueous solution(2 mM) and by using the platinum wire as the counter electrode anodic oxidation was executed on the condition described bellow. The dependence of the flow rate of solution on the current of oxygen reduction was investigated using obtained sensor. Namely, the beaker with magnetic stirrer was filled by a saline, and the above-mentioned sensor was used as the working electrode and the silver/silver chloride was used as the counter electrode, then the solution was contacted with air at the room temperature to be saturated with air.

The negative voltage of 0.6 volt(vs Ag/AgCl) was applied at the working electrode, and the flowing cathodic current



(SEM), the depth of the etched part of carbon fibers was about 100  $\mu\text{m}$ , and the surface of the electrode was sharp like a pencil.

The thin layer of platinum was made on the above-stated micro-hole electrode by the method which is explained hereinafter. Namely, the micro-hole electrode was dipped in the aqueous solution containing chloro-platinic acid (0.037 mol./l), ammonium phosphate (0.134mol./l) and sodium phosphate (0.704mol./l), and the current was run to the amount of 8 mC using platinum as the counter electrode. Then the electrode obtained was well washed with deionized water. On the observation by SEM, the platinum thin layer of about 0.6  $\mu\text{m}$  adhered on the electrode uniformly.

The FIG. 3 showed that the progress of the electrode contamination when electrode after plating with platinum (represents "Platinum" in the FIG.) and electrode before plating with platinum (represents "Carbon" in the FIG.) were left in the LB culture composition (37°C).

The carbon electrode was shown by dotted line and the platinum electrode was shown by solid line. The each lower line showed the value that the electrode didn't have micro-hole and upper line showed the value that the electrode had micro-holes, the depth of which was about 100  $\mu\text{m}$ . In each case, the descending rate of oxygen

The same electrode as of Example 1 was made except that the diameter of the carbon fiber was  $5\mu\text{m}$ .

The burnished part was dipped in the sulfuric acid aqueous solution(2 mM) using the platinum wire as the counter electrode and it was oxidized electrochemically at the constant current of 0.2 mA. The carbon fibers were etched about  $100\mu\text{m}$ . Then it was standing at -0.7 volt for 20 minutes.

Similarly, the electrode of carbon fiber etched about  $100\mu\text{m}$  was made, using each bundle of one hundred fibers having diameter of  $20\mu\text{m}$  and  $30\mu\text{m}$  respectively.

Negative charge (-0.7v) was applied at this each electrode using the electrode of silver/silver chloride as the counter electrode in the solution of LB culture composition. The descending rate of oxygen reduction current was obtained after 24 hours. The result is shown in Table 2. This descending rate is small when the micro-hole is small.

TABLE 2

the diameter of carbon fiber ( $\mu\text{m}$ )	the descending rate of oxygen reduction current (%)
5	10
7	15
20	35
30	50

**Example 6**

Each electrode was made by the same method as Example 4 except using phenol, 2,5-dimethyl phenol, 4,4'-diamino-diphenyl ether instead of aniline. Though it was left in LB culture composition at 37°C for 10 days, the descent of the value of the oxygen reduction current wasn't observed.

**Example 7**

The bundle of three thousand carbon fibers ("Torayca T-300", having the diameter of  $7\ \mu\text{m}$ ) was put into the polyethylene tube (inside diameter was 2 mm) of 35 cm length, and one end of carbon fibers was fixed at outside of the tube. The epoxy resin (produced by Toray-Hysol Co. Ltd.,) containing hardening agent was poured from the inlet where the carbon fibers were fixed. This was post-

cured on about 60°C for one hour and a half, then hardened carbon fiber composite material was pulled out from the tube, and cut into 10 cm length. Next, it was treated with heat by electric furnace. One end of this carbon fiber composite material was bonded to the lead wire by silver paste, and another end was burnished by means of conventional method after the side face was insulated completely by epoxy resin.

The part of carbon fibers were removed by anodic oxidation of this electrode in sulfuric acid aqueous solution( 2 mM) using platinum plate as the counter electrode. The anodic oxidation was done at constant current 1 mA for 10 minutes and twenty minutes respectively. The depth of micro-hole was  $90 \mu\text{m}$  at 10 minutes, and was  $140 \mu\text{m}$  at 20 minutes. Negative charge (-0.6v) was applied at this electrode in a saline by using silver/silver chloride as the counter electrode, then the value of dissolved oxygen reduction current was measured. Thereafter the value of the current when the solution was stirred, devived by the current when it stopped was obtained. The values were 1.57, 1.34 respectively when anodic oxidation was done for 10 and 20 minutes.

## Example 8

The composite material of carbon fiber and epoxy resin was made as similarly as Example 1 except that the number of fibers was three thousand. When this carbon fiber composite material was oxidized anodically at constant current (1 mA) in the sulfuric acid aqueous solution( 2 mM) using platinum plate as the counter electrode, the carbon fibers were etched about  $200 \mu\text{m}$ . Next, plating with platinum was done on the carbon fibers like Example 4 by the amount of 12 mC.

The temperature dependance of the value of oxygen reduction current at this electrode was less than 0.8 %/ $^{\circ}\text{C}$ . This value was smaller than that of Clark oxygen sensor which was in the range of from 4 to 5 %/ $^{\circ}\text{C}$  (Cf. "The optimum measuring and control of the fermentation process". Science Forum Page 214).

The end of this electrode was dipped in polyvinyl chloride (produced by Kanto Chemical Co. Ltd.,) 8 wt% solution (dimethylformamide), and it was left in methanol for 3 hours. Then after it was washed well by the deionized water, it was left in 20 cc of phosphate buffer solution (0.066M) containing glucose oxidase 5 mg (produced by Nagase Co. Ltd.,) for 10 hours. It was washed by deionized water, and -0.6v was applied (vs.SCE) in phosphate buffer solution (0.066M) using the saturated

calomel electrode as reference electrode and platinum wire as the counter electrode. At this time, the relationship between the concentration of glucose and the decrease of oxygen reduction current was linear. It took sixty seconds for the current to become constant. The changed rate of the current by temperature change of the solution was 1.4%/°C.

When the potential( which was applied at this enzyme electrode) was changed to +0.6V (vs. SCE), the relation of the glucose concentration and oxidation current (current of hydrogen peroxide oxidization) was good linear relationship by our investigation.

#### Example 9

The carbon fiber composite material was made by same method as Example 8, and the carbon fibers were etched about  $200\text{ }\mu\text{m}$ . And at once it was dipped in 20 cc of phosphate buffer solution (0.066M) containing the glucose oxidase 10 mg for 10 hours. It was washed well by deionized water, and the relation of the glucose concentration and the amount of the decrease of oxygen reduction current like Example 6 was a straight line passing zero point. The changed rate of current by temperature change of solution was 1 %/°C.

**Example 10**

The carbon fiber composite material was formed using the bundle of one thousand carbon fibers ("Torayca T-300", having the diameter of 7  $\mu\text{m}$ ) like Example 1.

This composite material was oxidized electrochemically at constant current (0.34mA) in the sulfuric acid aqueous solution(2 mM), and anodically etched about 200  $\mu\text{m}$ .

A polymer membrane was electrochemically deposited at 1.5 volt (vs. SCE) for 10 minutes in acetonitrile solution containing 2,6-dimethylphenol (20mM) and sodium perchlorate (0.2M) using platinum wire as the counter electrode, and saturated calomel electrode as the reference electrode. The potential in various pH solution was investigated by using this electrode and good linear relationship with the inclination of -56 mV/pH was obtained. It responded in 1 minute when the electrode was removed from pH2 solution to pH10 solution.

**Comparative Example 2**

The constancy of potential was investigated by using the same pH electrode as Example 10 and the same one (except without micro-hole) in the phosphate buffer solution which includes the yeast extract essence (0.5 wt%), bactotryptone (0.3 wt%). As the result, the electrode with micro-hole gave the stable potential, but that of without micro-hole

gave the potential slip, its error was 5 mV.

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Example 11

The same electrode except that the depth of etching was  $100 \mu\text{m}$  was formed. This electrode was plated with platinum by the amount of 4 mC as described in Example 4.

A polymer was electrochemically deposited on this electrode at 1.0 volt (vs. SCE) potential in the phosphate buffer solution( 2 M, pH=7) which contains 1,2-diamino benzene (20mM) for 10 minutes, using platinum wire as the counter electrode and saturated calomel electrode as the reference electrode. As by using this electrode the potential was investigated in solutions having various pH value, good linear relation having the inclination of -53 mV/pH was obtained during pH4 and pH9.

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INDUSTRIAL APPLICABILITY

The minute electrode of this invention is useful for various electrode of electrochemical analysis, and it is suitable especially for the electrode for measuring the concentration of dissolved oxygen, for the concentration of ions, for bio sensor, or for the reference electrode.

## CLAIMS

1. Minute electrode for electrochemical analysis characterized in that it is comprised of the bundle of carbon fiber coverd with the nonconducting resin and the end of carbon fiber recesses from one end of the resin and the micro-hole which is released to the outside is formed.
2. The minute electrode according to the CLAIM 1, wherein the diameter of carbon fibers is less than  $20 \mu\text{m}$ .
3. The minute electrode according to the CLAIM 1, wherein depth of the micro-hole is in the range of from 0.5 to 500  $\mu\text{m}$ .
4. The minute electrode according to CLAIM 1, wherein nonconducting resin is selected from the group of high molecule material, fluorinated resin, polyester resin, epoxy resin, polyphenylene oxide resin, polyphenylene sulfide resin, urethane resin, silicon resin, vinyl chloride resin, phenol resin.
5. The minute electrode according to CLAIM 1, wherein

surface of the end of recessed carbon fiber is covered  
with selective permeable membrane.

6. The minute electrode according to CLAIM 5, wherein  
selective permeable membrane is electropolymerized  
membrane.

7. The minute electrode according to CLAIM 6, wherein  
electropolymerized membrane doesn't have electroactivity  
for the measuring the concentration of dissolved oxygen.

8. The minute electrode according to CLAIM 6, wherein  
electropolymerized membrane responds the hydrogen ion for  
measuring concentration of ions.

9. The minute electrode according to CLAIM 1, 2, 3, 4, 5,  
6, 7 and 8, wherein the enzyme and microorganism are  
immobilized near the end of recessed carbon fiber.

10. The minute electrode according to CLAIM 1 for  
reference electrode, wherein the surface of the top of the  
recessed carbon fibers are covered with silver, and they  
are covered further with silver halide thereon.

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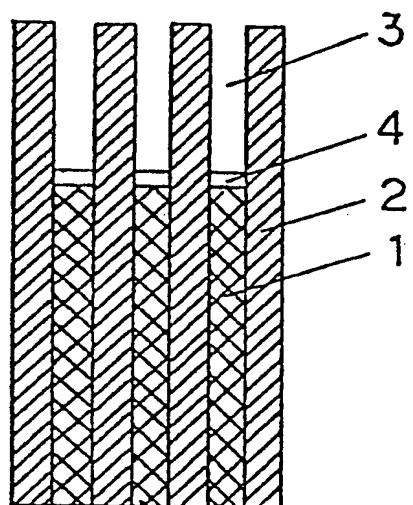


FIG. 1

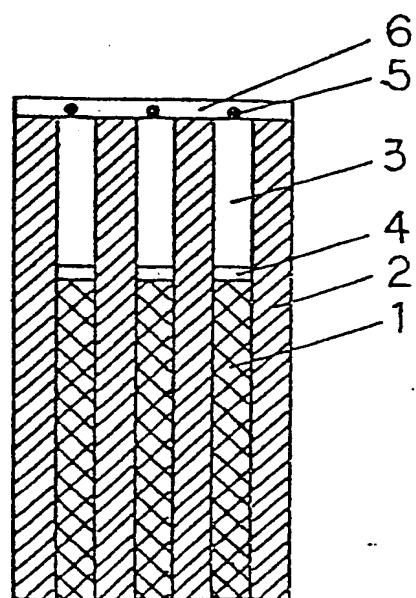
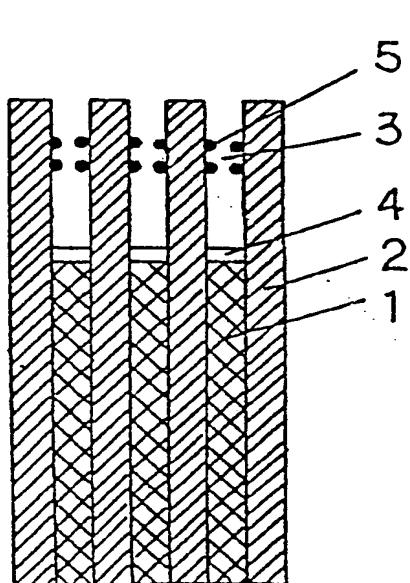


FIG. 2

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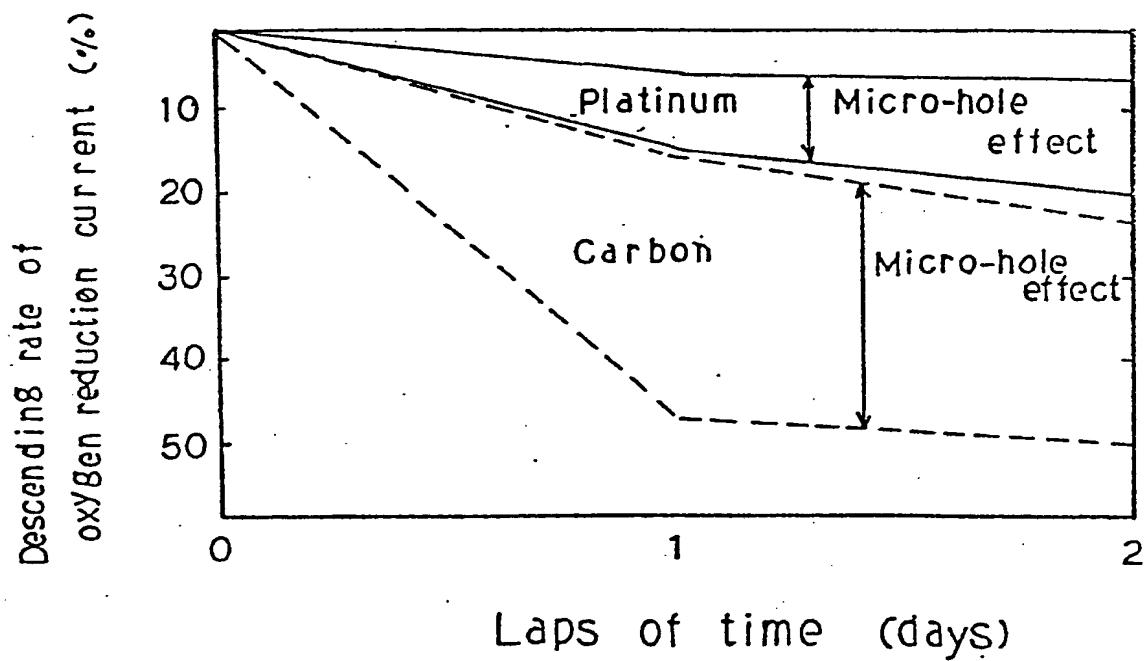


FIG. 3

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## INTERNATIONAL SEARCH REPORT

International Application No.

PCT/JP87/00252

## I. CLASSIFICATION OF SUBJECT MATTER (If several classification symbols apply, indicate all):

According to International Patent Classification (IPC) or to both National Classification and IPC

Int.C1<sup>4</sup> G01N27/30

## II. FIELDS SEARCHED

Minimum Documentation Searched<sup>4</sup>

Classification System | Classification Symbols

IPC

G01N27/30, 27/46-27/56

Documentation Searched other than Minimum Documentation  
to the Extent that such Documents are Included in the Fields Searched<sup>5</sup>Jitsuyo Shinan Koho 1926 - 1987  
Kokai Jitsuyo Shinan Koho 1971 - 1987III. DOCUMENTS CONSIDERED TO BE RELEVANT<sup>14</sup>

Category <sup>6</sup>	Citation of Document, <sup>15</sup> with indication, where appropriate, of the relevant passages <sup>17</sup>	Relevant to Claim No. <sup>18</sup>
A	JP, A, 60-52759 (Terumo Corporation) 26 March 1985 (26. 03. 85) (Family: none)	1-10
A	JP, A, 60-77984 (Rikagaku Kenkyusho) 2 May 1985 (02. 05. 85) (Family: none)	1-10
A	JP, A, 61-7463 (Murai Teiichi) 14 January 1986 (14. 01. 86) (Family: none)	1-10

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## IV. CERTIFICATION

Date of the Actual Completion of the International Search<sup>19</sup>

July 7, 1987 (07. 07. 87)

Date of Mailing of this International Search Report<sup>20</sup>

July 20, 1987 (20. 07. 87)

International Searching Authority<sup>21</sup>

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